

**Development of a high performance transtibial cycling specific  
prostheses for the London 2012 Paralympic Games**

Bryce Dyer<sup>1</sup>

Howard Woolley<sup>2</sup>

<sup>1</sup>Bournemouth University, Poole, UK

<sup>2</sup>Pace Rehabilitation, Cheadle, UK.

**Corresponding Author:** Bryce Dyer, Faculty of Science & Technology,  
Bournemouth University, Poole, BH12 5BB, UK. [brdyer@bournemouth.ac.uk](mailto:brdyer@bournemouth.ac.uk)

## **Abstract**

### ***Background and Aim***

It has been reported that cycling-specific research relating to participants with an amputation is extremely limited in both volume and frequency. However, practitioners might participate in the development of cycling-specific prosthetic limbs. This technical note presents the development of a successful design of a prosthetic limb developed specifically for competitive cycling.

### ***Technique***

This project resulted in a hollow composite construction which was low in weight and shaped to reduce a rider's aerodynamic drag.

### **Discussion**

The new prosthesis reduces the overall mass of more traditional designs by a significant amount yet provides a more aerodynamic shape over traditional approaches. These decisions have yielded a measurable increase in cycling performance. Whilst further refinement is needed to reduce the aerodynamic drag as much as possible, this project highlights the benefits that can exist by optimising the design of sports-specific prosthetic limbs.

**Word Count of Abstract:** 141

### **Keywords**

*Prostheses design, amputation, cycling*

### **Clinical Relevance**

~~This project resulted in the creation of a cycling-specific prosthesis which was tailored to the needs of a high-performance environment. Whilst further optimisation is possible to yield further~~

gains, this new design provides insight into the design and development of sports-specific prosthetic limbs.

This project resulted in the creation of a cycling-specific prosthesis which was tailored to the needs of a high-performance environment. Whilst further optimisation is possible, this project provides insight into the development of sports-specific prostheses.

**Word Count of Clinical relevance: 44**

## **Background and aim**

A recent review of the literature has revealed that both research and clinical experience is extremely limited<sup>1</sup> to help guide prosthetists with the creation of cycling specific prostheses. A traditional prosthesis used for walking can be used for cycling but falls short of two key performance indicators crucial to competitive cycling.

The first is to realise the importance of aerodynamics when cycling competitively by lowering the aerodynamic drag<sup>2</sup>. This even applies to components as proportionally as small as a prosthetic limb<sup>3</sup>. Kyle & Burke<sup>6</sup> recommended a hierarchy for addressing the reduction of aerodynamic drag as:

- Reducing the frontal area
- Streamlining the geometry

- Lowering the surface roughness.

The second goal is to reduce the prosthetic mass as this will reduce the energy the rider will have to expend when accelerating or climbing.

The aim of this technical note is to present and discuss a case study of a high performance cycling prosthetic limb design undertaken for the London 2012 Paralympic Games. Both participant consent and institutional ethics were obtained prior to this project.

## **Technique**

### *Participant*

A male, international-level cyclist (age=34, height=1.72m, weight= 73kg) acted as the participant for this case study. The participant had been using a walking prosthesis to cycle prior to this project. Due to a neurologically related disability, the athlete lacked full ankle control of their sound limb.

### *Design Specification*

The athlete wished to use the limb to compete across a diverse range of cycling events including the track-based 1km time trial and 4km individual pursuit

events plus the 20km outdoor 'individual time trial'. However, the nature of these events is very different. The track time trial requires maximum effort from a stationary standing-start position to complete the event. Conversely, both the individual pursuit and the individual time trial require a more evenly distributed steady-state power output. As a result, the prosthetic solution needed to accommodate this diverse range of needs.

Prior to the design process, the key constraints of the prostheses design were sourced from peer reviewed literature and the prostheses manufacturer. A summary of these criteria is in table 1.

[INSERT TABLE 1]

### *Prosthesis Fit*

The way the prosthesis is attached to the cyclist is a critical factor in achieving an efficient power transfer. This connection must be as rigid as possible whilst at the same time being comfortable for the duration of the competitive event. A Sealin X5 liner (Ossur) with valve (Ossur A-551002) was selected as the suspension system. The starting point for the length and alignment of the diagnostic prosthesis was produced by taking a profile of the cyclist's sound side in the sagittal plane with the foot in a plantar flexed (toe down) position. A

measurement was taken from the patella tendon to the centre of the cycling cleat. This established the initial socket to cleat position. To help with this process in the clinic, the participant used a stationary trainer (a product which attaches a bicycle in a stationary position and allows it to be ridden). Minor adjustments were then made to the length and alignment using a diagnostic prostheses which is adjustable in six different degrees of freedom and whose measurements would then be transferred to a jig. This jig would place a mandrel inside the proposed socket and lock it in position between both this and the pedal cleat. This would serve as the guide for the final prostheses. The cyclist subsequently undertook field trials by riding their bicycle in a velodrome at exercise intensities commensurate with the power output experienced in their racing. Qualitative feedback and expert observation contributed to the designs refinement. Key observations during these trials are shown in table 2.

[INSERT TABLE 2]

### *Prostheses Form Design*

An aerofoil form was selected for the pylon region. It has been shown that aerofoil based bicycle frames offer considerably less drag than a round tube traditional design<sup>2</sup>. To determine which aerofoil profile was most suitable for this

application, an accurate measurement of the near vertically angled seat tubes from contemporary wind tunnel validated bicycle frames was undertaken. However, it is conceded that there is some angular variation of the lower-leg when cycling.

The aerofoil design was modified further through addition of a Kamm profile. The Kamm concept has been used extensively in both the automotive and aeronautical industry and its definition is that of an aerofoil that is cut when the rear taper reaches 50% of the aerofoils maximum width. This concept has recently been applied to bicycle frame member design<sup>7</sup>. The Kammback principle allows a cut aerofoil to obtain nearly the same aerodynamic performance as an uncut aerofoil. Whilst the optimisation of this profile would require more than a casual application of aerodynamics, it was felt that the design would also provide beneficial levels of lateral and torsional stiffness over that of a traditional aerofoil<sup>7</sup>. This would be of extra benefit to the higher forces of the athlete's track time trial event. The Kamm width at its narrowest point was defined as the thinnest that the fabrication process was deemed to feasibly achieve and was 36mm in thickness with a 108mm aerofoil depth. The aerofoil was tapered further down the pylon area to meet the smaller shape and size of the cleat/foot area.

It is likely that an optimal aerofoil design would be different between indoor and outdoor use but the Kamm design was not specified for a specific wind yaw. Yaw is the net angle of the net air flow that strikes the cyclist and is dictated by riding speed and any external wind speed. In the case of this project, the athlete would only have one prostheses so a conservative approach to the aerofoil design was taken. Either way, the Kamm design has been shown to be beneficial in wider ranges of wind yaw<sup>7</sup>.

### *Limb Construction*

The prostheses shank and foot region was shaped and manufactured by hand from high density foam. Templates were used to provide cross-sectional dimensional consistency of the shank and a mid-construction example of the composite being applied over the shaped foam core is shown in figure 1.

[INSERT FIGURE 1]

A composite construction was then created using three layers of multi-directionally applied 6k carbon fibre with orthocryl laminating resin. Once this was complete, the foam core was removed by boring the foam out using a tool inserted where the cleat would be mounted and by cutting down the centre of



the Kamm rear face to remove the foam higher up. This cut would then be re-joined by re-laminating it afterwards. The rotational alignment of the aerofoil was achieved through use of a jig that aligned it exactly perpendicular to the cycling pedal cleat. This stresses the importance of establishing the optimal position of the pedal cleat, prior to final prostheses construction. The cleat threaded inserts were bonded through the laminated face of the underside of the foot and reinforced using an aluminium metal plate that was imbedded between the three layers of carbon fibre. Some natural reinforcement was created when the cloth was neatly folded around key areas.

## **Results**

The participant's first generation limb possessed a mass of 1.86Kg. The mass of this prosthetic leg was 0.72Kg, resulting in a reduction in mass of around 1kg. An image of the completed limb is shown in figure 2a, 2b and 2c.

[INSERT FIGURES 2A, 2B AND 2C]

## **Discussion**

Since this project's completion, aerodynamic drag measurement has now been applied to a similar design to this limb for the 2016 Paralympic Games and has yielded a potential 23 second time saving over a conventional round shank design when performing a 16.1km time trial. Within two months of this project's completion, the cyclist won the 2012 World Cycling Time Trial Championships in their disability category.

A 1Kg reduction in mass was a significant saving over the user's previous prostheses and reduced the total mass needed to be accelerated from rest in a standing start by approximately 1.1%. For future designs, further improvements in prostheses mass and aerodynamic drag could be made through the use of pre-preg carbon fibre. This would potentially reduce the profile of the blade area and reduce the mass whilst maintaining the required strength and rigidity.

It could be suggested that an optimised design could have been generated using computational fluid dynamics (CFD). However, it is not known what impact any airflow interaction and interference of the leg and bicycle would have on each other and CFD would have to model an exact reproduction of the specific rider and their equipment. This might prove to be an innovative approach in the future but may be cost prohibitive when in comparison to field testing. Field testing proved essential as the cleat and socket alignment

required adjustment that was only apparent when the participant performed trials on their own bicycle at power outputs typical of their specific events. With this in mind, cost-effective field testing methods for this purpose have been formally validated<sup>3</sup>.

### **Key Points**

- An aerofoil is aerodynamically superior to a round tubed section.
- Reduction of the excess mass of a prostheses is essential for cyclists to reduce their energy expenditure.
- Any prosthetic fit or evaluation should be conducted using exercise intensities consummate of the athlete's chosen events.

### **Author contribution**

All authors contributed equally in the preparation of this manuscript.

### **Declaration of conflicting interests**

Institutional ethics approval was obtained for this project.

### **Funding**

Any associated costs for this project formed part of pro bono assistance given to the participant and were fully underwritten by the author's employers.

**Main text word count: 1483**

### References

1. Dyer B. Cycling with an amputation: A systematic review. *Prosthetics and Orthotics International* 2015; DOI:0309364615610659.
2. Lukes R, Chin S and Haake S. The understanding and development of cycling aerodynamics. *Sports Engineering* 2005; 8: 59-74.
3. Dyer B. The importance of aerodynamics for prosthetic limb design used by competitive cyclists with an amputation: an introduction. *Prosthetics and Orthotics International* 2014; doi: 10.1177/0309364614527121.
4. UCI, *Clarification of the UCI technical regulation*  
[http://www.uci.ch/mm/Document/News/Rulesandregulation/16/51/61/ClarificationGuideoftheUCITechnicalRegulation-15.01.2016-ENG\\_English.pdf](http://www.uci.ch/mm/Document/News/Rulesandregulation/16/51/61/ClarificationGuideoftheUCITechnicalRegulation-15.01.2016-ENG_English.pdf) (2016, accessed 2/2/16).
5. UCI, Paracycling: Integration and Approval. *Update Sport and Technical* 2013; 6:9.
6. Kyle C and Burke E. Improving the racing bicycle. *Mechanical Engineering* 1984; 106: 34–35.
7. Harder P, Cusack D, Matson C, and Lavery M. Airfoil Development for the Trek Speed Concept Triathlon Bicycle. *Trek Bicycle Corporation*,  
[http://www.cyclescience.com.au/Members/carl/TK10\\_SC\\_white\\_paper\\_lores.pdf](http://www.cyclescience.com.au/Members/carl/TK10_SC_white_paper_lores.pdf) (2010, accessed 12 December 2011).

